Pharmaceutical Glass Interactions: A Review of Possibilities

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Abstract
Glass is used as packaging material for parenteral formulation from years. Various untoward occurrences have observed over the period of time with glass containers which leads to therapeutic failures or even toxicity to the patients. Glass has been the primary choice for packaging of parenteral formulations, unexpected degradation or product losses during stability have forced many researchers to evaluate the underlying mechanisms leading to a larger understanding of some of the untoward properties of glass. Oxides of various metal ions viz. aluminium, arsenic, barium, iron etc. are added in glass to modify its physico-chemical properties based on specific requirements. Metal ions could leach from the glass structure due to several reasons and could lead to generation of particulate matter, could cause metal ion toxicity or act as catalyst to hasten drug degradation. Delamination or formation of glass flakes is one of the major problems currently under high scrutiny by the regulators. Similarly, some molecules have an affinity to adsorb to glass leading to a low potency in the administered drug. Interaction between glass and drug product depends upon composition/type of glass, processing of glass and formulation variables such as pH, buffer, properties of drug, sterilization cycles, storage conditions etc. This review describes several possible means of interaction of glass and drug product encountered by researchers under a gamut of conditions.

Keywords: Glass, delamination, leachables and extractables, particulate matter.

Abbreviations:
Al (aluminium), As (arsenic), Ba (barium), Fe (iron), Ca (calcium), Mg (magnesium), Mn (manganese), Si (silica), SiO2 (silicon dioxide), B2O3 (boron oxide), P2O5 (phosphorus oxide), GeO2 (germanium oxide), Fe3O4 (Ferric oxide), TiO2 (titanium oxide), MnO (manganese oxide), NaCl (sodium chloride), KCl (Potassium chloride), MgCl2 (magnesium chloride), ZnSO4 (zinc sulphate), ETAAS (electrothermal atomic absorption spectroscopy), AAS (atomic absorption spectroscopy), SEM (scanning electron microscopy), ICP-OES (inductively coupled plasma optical emission spectrometry).

INTRODUCTION
Wide ranges of packaging material are being used for different types of dosage forms. Selection of packaging material mainly depends on:

- Type of dosage form
- Mode of application
- Physico-chemical properties of formulation being packed into
- Physico-chemical properties of material being used for packaging

Regulatory requirements also vary with the intended application of the drug product like for e.g., packaging for parenteral products poses stringent regulatory requirements since sterility is a major concern there [1]. FDA also recommends specific quality controls and requirements of packaging components based on intended use of dosage forms. Glass containers have been widely used for packing of parenteral preparations since many years. Glass containers are widely used in pharmaceutical industry but cannot be considered completely inert. Various interactions could arise when products come in contact with glass surfaces including leaching, ion exchange, precipitation, glass dissolution, surface layer exfoliation, and corrosion [2]. Various authors have reported different potential leachables from glass containers and effect of formulation and process factors on total leachables. The purpose of this article is to present a consolidated review of such reported interactions of glass with the drug product leading to a stability challenge and/or a potential or obvious toxicity to the patient.

Glass: As pharmaceutical packaging component
Commercial glasses are an inorganic material (mostly silicates) or mixture of materials that have been heated to a molten liquid state then cooled without crystallization to a solid state. Several metallic oxides have the property to cool without crystallization, e.g. SiO2, B2O3, P2O5 and GeO2. These oxides are used as backbone in glass. SiO2 is the most commonly used oxide including containers for sterile dosage forms [3].

Mechanism of glass formation
Silicate glasses are made up of SiO4 (tetrahedral form of Si), in which each Si atom attached with four oxygen atoms and each oxygen has bonding with two Si atoms via covalent bonds. Due to this type of 3-D arrangement and spatial interactions, viscosity of the melted silicates increase rapidly during cooling phase which do not allow the transition from random structure of liquid state to ordered crystalline structure [3, 4].

Types Of Glass
Various minerals are added to improve the industrial feasibility and physical properties of the glass. Based upon
the minerals which are incorporated, glass families are broadly classified into two [5, 6]:

A. Soda-lime-silicate glasses or Soda-lime glasses
In this type of glass, soda ash (sodium carbonate) and lime stone (calcium carbonate) are added as a source of sodium oxide and calcium oxide respectively to modify the properties. These comprise of 25% by weight. Magnesium and potassium may be used as their oxides to reduce the melting point. Soda-lime glass has poor chemical resistance because of chances of leaching of mobile nature of sodium and potassium cations.

$\text{Al}_2\text{O}_3$ is added to improve chemical durability of the glass because $\text{Al}^{3+}$ ions are able to form covalent bonds and hence, more resistant to leaching. $\text{Fe}_2\text{O}_3$ is added to provide light protection. It absorbs ultraviolet wavelengths more effectively than colourless glass [3].

B. Borosilicate glasses
$\text{B}_2\text{O}_3$ is used in replacement of some sodium and Ca ions. Borosilicate glasses have exceptional chemical durability, high heat resistance- including resistance to sudden temperature changes and thermal shock. Borosilicate glasses are most commonly used for parenteral containers due to its high resistance to thermal processes including depyrogenation, lyophilization and terminal sterilization and low alkali extractable. $\text{Fe}_2\text{O}_3$ and $\text{Ti}_2\text{O}_3$ or MnO can be added to produce amber borosilicate glasses for protection from ultraviolet light.

**Mechanism Of Interaction Of Glass With Product**

A. Ion exchange
Ion exchange is the most important mechanism of interaction between glass and product. $\text{Na}^+$ ions which are present in glass can be replaced by the $\text{H}_3\text{O}^-$ ions of the solution. This reaction is dominant in neutral and acidic solutions.

B. Attack on glass by reactive groups
Hydroxyl groups and alkaline species present in product as well as glass itself can attack the glass leads to breaking of $\text{Si-O}$ bonds. This reaction depends upon various factors like glass formulation, pH of product, ingredients of product etc. e.g. chelating agents are more aggressive toward glass because they are able to pull the various metal ions out of the surface. It means guidelines for selection of glass for parenteral products based on pH alone are not sufficient.

C. Additional mechanisms
Process involved in manufacturing of containers has effect on composition and physico-chemical parameters of the surface. e.g. during manufacturing of ampules and vials, the temperature of inner surface can exceed the boiling point of low boiling point ingredients, mainly sodium and boron. During cooling, they could condense as sodium borate. Complete removal of sodium borate from containers may not be possible during washing of containers. This alkaline residue can again affect the product by three mechanisms: Firstly, this alkaline residue may react directly with product. Secondly, exchange of $\text{Na}^-$ ions with $\text{H}_3\text{O}^-$ ions, loss of $\text{H}_3\text{O}^-$ ions in the solution can increase the pH of product. Thirdly, in extreme cases, the interaction can trigger the formation of an unstable layer of silica gel which can slough off as delaminated glassy particles

Irrespective of the type, all glasses have the potential to leach alkali related components into the product upon storage which may affect the stability of that product and this varies depending on storage conditions, type of glass used for the storage, type and nature of the product being stored. There is high probability of more leachable content coming into the product at higher pH i.e., pH > 9. Most common extractables from glass includes silicon, sodium, and boron which take major part in contamination and/ or degradation of drug product [4].

Despite of the presence of various inorganic leachables viz. Al, Si, B, Ba ions etc. and interaction with different buffers viz. acetate, citrate, phosphate etc. glass is most widely used packaging material for parenteral formulations. Glasses can be modified by various techniques to better suit the formulation like amber colour glass for photo sensitive drugs. Selection of glass and the type of modification depends upon the formulation and storage.

Some researchers showed that elements of the drug and formulation variables like pH, buffers etc. causes degradation of glass, ultimately contaminating the product which leads to adverse effects in patients. Amount of various ions which could leach in the formulation varies depending upon the affinity of drug and (or) excipients for specific ions.

In this paper, we have broadly classified major probable mechanisms of drug product contamination by glass into 4 categories:

A. Glass delamination
B. Metal ions interaction
C. Interaction with buffers
D. Adsorption of drug(s) or formulation components on glass surfaces

A. Glass delamination or generation of glass flakes
Glass delamination or generation of glass flakes is a major concern with parenteral products that use glass vials for their storage and these glass flakes may or may not be visible for direct inspection and the products which contain these glass particles when injected directly may lead to embolic, thrombotic and other vascular events [7]. Possible reasons contributing to glass delamination is [8, 9]: (i) Differences in manufacturing process of glass vials i.e., moulding or formation from glass tubing - higher chance of delamination is associated with vials produced by tubing process due to the utilization of higher temperatures during production. (ii) Nature of formulation being stored - Alkaline and certain buffer solutions (citrate and tartrate) have higher tendency to aggravate the process of delamination (iii) terminal sterilization process (iv) Presence or absence of ammonium sulfate coating on inner surface of glass vials where the treatment with sulfur enhances the chances of delamination (iv) Storage duration and storage conditions - Storage at room temperature is believed to have higher chance of glass delamination over cold storage conditions.

Glass manufacturing process differences and the nature of product seem to be the most dominant factors that enhance glass delamination characterized by pH changes, active moiety degradation, formation of visible particles and
increased extractable levels ultimately affecting the product quality adversely. Ronald, et al., investigated the delamination/corrosion of glass by a pharmaceutical product having pH of 8.2. Authors have used three type-I borosilicate glass vials from two different vendors of which two vials (ammonium sulfate treated and the other one un-treated) were kept in contact with the product with pH of 8.2 and the remaining were used as a control. Vials were stored under 2 different temperature conditions 40°C and 30°C. Visible particulate matter was observed in vials contained product after 30 days and 8 weeks of storage at 40°C and 30°C respectively. The particulate matter was found to be glass as identified using field-emission environmental SEM equipped with X-ray analysis capabilities [9].

Richard, et al., investigated the effect of formulation and process variables on the delamination process. They also studied the impact of the glass manufacturing process, supplier, and glass surface treatment on delamination process. They used Type 1 borosilicate tubing vials from 3 different suppliers (total 18 lots) and studied the effect of formulation pH and moist heat terminal sterilization on delamination. They filled glass vials with Vistide® Injection (75 mg/mL, cidofovir in Water for Injection, USP) and to study the impact of pH, solutions pH were adjusted to pH 6.0, 7.0, 7.4, 8.0, and 8.5 with sodium hydroxide or hydrochloric acid. The filled vials were subjected to either one or three sterilization cycles (123°C for 19 min) following which the vials were charged on stability at 25°C, 30°C (real-time storage condition) and 40°C (accelerated testing condition). They monitored the delamination by visual inspection, particulate matter quantification, light obscuration and microscopic methods. Vials that were stored at 40°C after autoclaving showed the presence of glass particles which could be visually seen and increased amounts of the same was seen with prolonged storage time, increasing pH, sulfate treatment and higher number of sterilization cycles. At the same time, differences in the behaviour were observed between suppliers and presence or absence of sulfur coating. Real time stability data indicated that presence or absence of visible glass particles mainly depends on glass type from various suppliers due to differences in processing conditions and composition of the glass. Visible particles were found to be containing silicon dioxide and sodium which are major components of type-I glass as determined by SEM/EDX [10].

Ronald, et al., investigated the factors contributing to delamination which was demonstrated using himpiric acid, glutaric acid and pemexetred and three type-I borosilicate glass vial types. The vial types studied were ammonium sulfate coated on its inner surface from one vendor, and other two vials sourced from different vendors where one vial type was uncoated and other type contained silicon dioxide coating. Empty vials were initially subjected for depyrogenation at 250°C, and 350°C followed by filling and sterilization of the filled vials by no or two terminal sterilization cycles at 122-125°C for 15min. The vials posts the treatments were stored at 5°C, 25°C, 40°C, and 60°C. pH measurements showed a decrease in pH values compared to initial high pH values (>8) and this decrease in pH was prominent at higher storage temperatures, the authors concluded that the drop in pH values was not because of degradation of test solution but because of degradation of glass itself. ICP-OES analysis revealed the presence of higher amount of Si in vials with ammonium sulfate treatment than that of silicon dioxide treated vials followed by uncoated vials. Presence of higher amount of Si in the test solutions is indicative of loss of glass durability or onset of glass delamination which may lead to formation of particulate matter or glass flakes. The authors have finally attributed the delamination to higher pH of product and anionic nature of test solutions at this higher pH [11].

Bisphosphonate dosage forms, e. g. Zoledronic acid solution can be administered intravenously as an infusion. These bisphosphonate dosage forms are highly sensitive to di-and polyvalent cations, especially Ca, Ba, magnesium, Al, boron, and silicon which are present in glass composition. Precipitate formation can be seen as a result of reaction between them which affect the quality of the final product and may cause severe toxicological problems. Formation of precipitation can be seen upon longer contact time of product with glass during storage or during terminal sterilization since sterilization process could enhance the leaching of metal ions from the glass containers. There are some marketed formulations which are lyophilized products of bisphosphonates that needed reconstitution before use where chances of precipitation are not absent because of presence of trace levels of metal ion impurities in saline solutions for infusion preparation. Alexandra, et al., took a step to address the current issue and invented a container that contains polymeric coating internally which is resistant towards the bisphosphonate drug solution. Moreover, the bottle itself can be terminally sterilized by which bisphosphonate drug solutions can be stored for prolonged time periods [12].

B. Metal ions interaction

Apart from delamination of glass surfaces, another important mechanism of drug product deterioration involves interaction with metal ions. Various metal oxides are added in glass during manufacturing process to impart physical and chemical properties. These metal ions including Al, As, Ba, Fe etc. have tendency to leach out and attack the product. Some important metal ion interactions are discussed here.

Aluminum

Al is the third most abundant mineral on earth and found in almost every animal and plant. It has been reported that most adults ingest between 3 and 5 mg Al daily which gets excreted in urine. However, Al is a body constituent; it is toxic if ingested in higher amount. Al toxicity was first reported in patients with chronic renal failure. Clinical manifestations include impaired bone growth in adults and delays in metal development in neonates. Parenteral nutrition is a considerable source of Al. Therefore, in July 2004, the FDA mandated manufacturers to include amount of Al in label. Limit of Al for large volume parenterals should be not more than 25 µg/L, for small volume
parenterals the label should state the potential maximum amount at expiry of the product. In cases where Al intake is more than 4–5 µg/kg/d in patients with impaired renal function, together with premature neonates, the label should include a warning that they may experience central nervous system and bone toxicity [13-15].

AI can easily get eliminated through urine however higher levels of AI pose significant risk problems to one’s body like bone growth impairment in patients with renal impairment and delayed mental development in neonates since the renal system is underdeveloped in neonates [13].

AI is a compositional part of glass and added during its manufacture as aluminium oxide and sometimes this may get leached into the product which is being stored in it and can contaminate the product. Few studies report the presence of AI in parenteral nutrition due to storage in glass containers. Content of AI increases with storage time and also depends on the nature of the substance in contact like, heparin and albumin. Product pH values at extremes also adversely affect the AI release.

Bohrer, et al., evaluated the amount of AI leached in parenteral nutrition containing amino acids. They used 19 amino acids and commercial nutrition formulation to check the effect of binding of amino acids from AI of glass material. They stored solutions of amino acids in type II glass flasks and AI content was measured periodically for 400 days by ETAAS. They concluded that the contamination with AI was observed with cysteine, cystine, aspartic acid and glutamic acid only. Leaching of AI from glass because of amino acids mainly depends upon stability of formed Al- amino acid complex i.e., higher the stability of complexes higher the ability of amino acids to release AI [16].

Toru, et al., studied the release of AI from borosilicate glass vials and the effect of different buffers like phosphate, citrate, acetate and histidine buffer at different pH on the release behaviour and precipitation of AI. The vials containing different buffer solutions showed the presence of AI and Si upon heating at any pH which demonstrated the ability of all buffers in extracting out the AI from glass containers and which depended upon concentration of solution, time of contact and storage temperature. Higher amounts of AI and Si were observed in glass vials with citrate buffer and in comparison to this lower amounts were observed with phosphate, acetate and histidine buffers. Upon storage particle formation was observed in phosphate and acetate buffers while no particulate matter was seen with citrate buffer which was attributed to its chelating property. This was supported by the reduction in AI content in phosphate, acetate and histidine buffer upon addition of AI ions during storage. At the end, the authors concluded that the possibility of formation of AI containing particles was much higher in phosphate buffer in comparison to other buffer solutions [17].

In an interesting study by Toru, et al., authors have investigated the characteristics of inorganic particles formed in phosphate buffer filled glass vials. Upon storage of the glass vials (which are compendially recommended for injectable products) filled with phosphate buffer, visible particles were seen and authors deliberated these particles to be different from delamination of glass. The particles comprised majorly of AI, P and O, however these particles were devoid of Si. With raise in temperature of the solution, particulate formation increased, these vials upon storage showed decreased amount of AI upon storage at 5°C for 6 months indicating the presence of AI in particles formed in the solution. Upon addition of AI chelating agent i.e., citrate there was effective reduction in the formation of the particles indicated the presence of interaction between leached AI from glass vials and phosphate buffer in the vials. This was further evidenced by the formation of white particles upon addition AI ions at concentration of more than 50ppb to the phosphate buffer. Sulfur treatment of inner surface of glass bottles provides a good mean to reduce the particle formation. Thus, great care needs to be taken for the storage of dosage forms containing phosphate buffer in glass containers [18].

Bohrer, et al., studied how the nature of substance can affect the AI release from glass containers. They evaluated the pharmaceutical products for parenteral use containing salts (sodium and potassium chlorides), glucose, heparin and albumin. All products were stored in glass and plastic containers. AI content was determined in glass as well as plastic containers at different storage time by AAS. They found that glass was the major contributor to AI content. Besides, AI contamination highly depended on the nature of substance which was in contact with glass surface. Table 1 shows the content of AI extracted by different substances after 60 days of storage [19].

<table>
<thead>
<tr>
<th>S.No.</th>
<th>Substance</th>
<th>AI content (µg/L)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1.</td>
<td>Salts</td>
<td>400</td>
</tr>
<tr>
<td>2.</td>
<td>Glucose</td>
<td>150</td>
</tr>
<tr>
<td>3.</td>
<td>Albumin</td>
<td>500</td>
</tr>
<tr>
<td>4.</td>
<td>Heparin</td>
<td>500</td>
</tr>
</tbody>
</table>

They found that all products stored in plastic containers contained not more than 20 µg/L of AI whereas in glass AI content reached 1000 µg/L and all of them showed an increase in AI content with age.

In another study, Bohrer, et al., evaluated the interaction of container and chemicals with glass container during heat sterilization. They stored 30 commercial solutions for parenteral nutrition in glass ampoules, in contact with rubber stopper and plastic container. All containers were subjected to heat at 121 °C for 30 minutes and AI content was determined. They found AI content of 1.57% in glass, 0.05% in plastic and 4.54% in rubber. Also, total AI released depended on the interaction of chemicals and containers. Various substances showed different AI content with glass ampoules and rubber stoppers and the data was shown in Table 2 [20].

They concluded that interaction of glass with chemicals (salts, acids and alkalis) could be explained by ion exchange properties, effect of formulation pH and affinity of chemicals especially amino acids for AI [20].
Based on available literature it is clear that glass can be a source of Al when products are being stored in glass containers but the extent of contamination may vary depending upon the type of product e.g. liquid form or powder form.

Marlei, et al., investigated the Al contamination in liquid and lyophilized forms of Erythropoietin which were contained in glass bottles sealed with rubber closures. The authors have found that glass and rubber were the sources of Al contamination after storage of formulation in contact with glass as well as rubber at 4 ± 2°C. As determined by atomic absorption spectrometry, higher Al contamination was found in glass vials with liquid formulation as compared to glass vials containing lyophilized form of the product. When stored in liquid form citrate and phosphate buffers extracted most of the Al present as contamination. The fact that glass container is a source of Al contamination can be supported by 19-fold increase in Al contamination after reconstitution in the same vials in 12 months as compared with the contamination before reconstitution. Moreover Al contamination after one month of reconstitution of lyophilized form is more than the contamination in lyophilized form after storage for 2 years in glass vials. The authors have concluded that lyophilized form of erythropoietin is preferred over its solution form for patients with chronic kidney disease [21].

Nakamura, et al., studied minodronic acid formulations having different compositions and their stability and tendency to generated particles upon storage at 60°C for 4 weeks. Upon characterization, the formed precipitate was found to be a complex between minodronic acid and Al ions apparently leached from the glass of the ampoules. The best protection in terms of stability as well as inhibition of particulate matter was afforded to formulations buffered by citric acid and tartaric acid, citrate buffer was better amongst the two particularly providing optimal results at a solution pH of 3 to 5 where no particulate generation was observed [22].

Further, the same authors demonstrated that a liquid formulation containing 0.5 mg/ml minodronic acid, 40 mM, pH 4.5, citrate, and sodium chloride stored in flint glass ampoules at 25, 40, 50, and 60 degrees C showed particulate matter generation at 25°C but not at higher temperatures. Analysis of the particulate matter by SEM/EDX revealed that the particulate matter contained Al and phosphorus. Storage in plastic containers and SiO2-treated glass ampoules did not show the rise in number of the particulate matter. A spike of minodronic acid solution with Al ions led to the particulate generation proving the interaction of minodronic acid molecules and Al ions to form a complex and resulting in particulate matter. Regular ampoules were found to be the source of leached AI [23].

### Table 2. Value of Al content in different products stored in contact with glass ampoules and rubber stopper

<table>
<thead>
<tr>
<th>S.No.</th>
<th>Substances</th>
<th>Container</th>
<th>Al content (µg/L)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1</td>
<td>Leucine, ornithine and lysine solutions</td>
<td>Glass ampoules</td>
<td>20</td>
</tr>
<tr>
<td>2</td>
<td>Solutions of basic phosphates and bicarbonate</td>
<td>Glass ampoules</td>
<td>1500</td>
</tr>
<tr>
<td>3</td>
<td>Cysteine, aspartic acid, glutamic acid and cystine solutions</td>
<td>Rubber stoppers</td>
<td>500</td>
</tr>
</tbody>
</table>

**Arsenic**

Transparency is one of the great properties which make glass suitable for packaging and storage of many of pharmaceutical products mainly in case of parenteral dosage forms. To make glass more transparent fining agents like arsenic oxide (III) may be added. This added arsenic oxide may get released out of glass into the product which is being stored under certain conditions like sterilization temperature and nature of substance. Released As can contaminate the product and upon intravenous administration it severely induces the toxic effects like skin ulceration, skin cancer, mucosal membrane damage, keratosis etc. [24]. Allowable limit of As species in products for IV administration should be less than or equal to 0.1 mg/L.

Bohrer, et al., in a study investigated the release of As (both As(V) and As(III)) from glass containers by action of intravenous nutrition formulation constituents after heating the ampoules at 121°C for 30min using hydride generation atomic absorption spectrometry (HG AAS). Before heating the ampoules containing nutrition formulation, As content of both the substances used in formulation as well as glass ampoules was determined and the results showed the presence of As (V) in higher amount in glass than As (III). This study indicated that during heating As is getting released from the glass containers and the solution composition decides the type and amount of As species getting released. Ampoules containing water for injection and solutions of NaCl, KCl, phosphates indicated the presence of As(V) only whereas ampoules containing amino acids, glucose, gluconate and vitamins showed higher concentration of As(III) since these can reduce the As(V) to As(III) due to their reducing behaviour [25].

Bohrer, et al., evaluated the presence of different As species (arsenite and arsenate) in several of the commercial parenteral formulations that included solutions of amino acids, salts, vitamins, and lipids and the measurements of As species were done using hydride generation atomic absorption spectrometry and results of which showed the presence of As in both the forms in all formulations. Presence of higher As contamination with varied ratios of As(V)/As(III) was evidenced in Calcium gluconate, sodium bicarbonate, heparin, and vitamin solutions. Interestingly the vials with water for injection and salt solutions showed only the presence of As(V) species but the ones with solutions of vitamins, gluconate, and glucose showed As(III) primarily the reason being the conversion of As(V) to As(III) since these sugars are reducing in nature. Evidence of the phenomenon was demonstrated by complete absence of As (III) in pure water and sodium chloride solution upon autoclaving for 15 minutes and occurrence of the same predominantly in solutions with reducing substances upon autoclaving [26].
Barium

Sam, et al., investigated the formation of barium sulfate crystals in six parenteral solutions that were packaged in both glass ampules as well as glass vials with rubber closures using a variety of micro analytical techniques. High melting point above 300°C indicated the inorganic nature of the barium sulfate crystals. Either drug molecule or the antioxidant appear to act as a source for sulfate ions which eventually reacts with the Ba ions which comes out from borosilicate glass and thereby results in formation of barium sulfate crystals which upon intravenous administration accumulate in different tissues and causes irritation [27].

Toshinobu, et al., evaluated parenterally administered aminoglycoside antibiotics i.e., micromonicin, sisomicin, tobramycin, and gentamicin for the presence of barium sulphate crystals. Glass ampoules containing aforementioned antibiotics with and without surface treatment were investigated for the presence of barium sulphate crystals using EDX. Results shown that higher faction of barium sulphate crystals were found in solutions of micromonicin than the other studied antibiotic solutions. In micromonicin solutions particulate content was observed to be increasing with increasing sterilization temperature, on the contrary no such increase was observed in case of surface-treated ampoules upon heating. Formation of these particles may be due to interaction between Ba from glass either with sulphate species of the composition or the sulphite antioxidants like sodium sulphite [28].

Bohrer, et al., have investigated the origin and extent of contamination of intravenous solutions with Ba for administration to neonates. Authors have tested several parenteral nutrition solutions that are commercially available and the administration kits for their contribution towards Ba contamination using atomic absorption spectrometry. As measured by AAS, some of the parenteral nutrition solutions highly contaminated with Ba were multivitamins, magnesium sulfate, and calcium gluconate solutions. Based on the data, the authors have concluded that leaching of Ba from containers contributed significantly in increased Ba contamination of products [29].

Iron (Ferric/ Ferrous)

Most of the glasses used for storage of parenteral products are transparent which allows passage of light through it. In cases where drug is photosensitive amber glass can be used which by nature inhibits the penetration of high energy light with a wavelength of less than 470nm thereby reducing the photolytic degradation of active substances [5, 30]. But amber coloured glass contains significantly higher quantities of Fe and Mn both of which reacts with the certain products being stored in it and resulted in degradation rather than stabilizing the formulation.

Enever, et al., studied the factors influencing decomposition rate of amitriptyline hydrochloride in aqueous solution. Amitriptyline hydrochloride is a photolabile drug and thus necessitates the storage of their solutions in amber colored bottles. Instead of being stable amitriptyline hydrochloride was getting degraded at much higher extent in amber color ampules in comparison to clear ampules. The authors found that the degradation by oxidation was a free radical-mediated process which was being enhanced by the presence of metal-ion contaminants. The source of these metal-ion impurities was found to be the amber coloured glass ampoules which contained higher Fe content than the clear glass ampules. Addition of 0.1% (w/v) edetate disodium prior to storage significantly reduced the decomposition rate [31].

Kassem, et al., and Lipper, et al., reported similar kind of degradation of ascorbic acid and thimersol in presence of metal-ions upon storage in amber coloured glass ampoules [30, 32, 33]. Reed, et al., determined the photochemical degradation of citrate buffered formulations of phenyl ether-based drug which were found to be light sensitive when studied according to ICH-defined light conditions though the molecule as well as the components of the formulation were not absorbing in the 300-700 nm exposure regions.

The pathway for degradation was proven to be interaction between Fe$^{2+}$ and dissolved oxygen to form superoxide radical when then protonated in water to generate hydroxyperoxyl radicals which eventually recombined to give hydrogen peroxide that reacted with Fe to give hydroxyl radicals. These hydroxyl radicals react with drug to produce phenol degrade. Fe levels present in the formulation were contributed by the raw materials used in the formulation as well as the glass vials, the amount of Fe for product being stored in glass increases with storage time and it could be due to Fe leaching from borosilicate glass vials. The combination of citrate from the formulation and light contributed to reduction of Fe. Thus, major contributors to the observed photosensitivity were the citrate buffer, parts per billion (ppb) levels of Fe, oxygen, and light exposure level. At a particular Fe concentration, formation of primary photodegradate was linearly proportional to the amount of light exposure. Moreover, at a fixed amount of light exposure, photodegradate formation was nearly linear proportional to the amount of iron (through 200 ppb levels) [34].

Quarry, et al., evaluated the degradation of compounds of the 4, 5-epoxymorphinan series (e.g. naloxone, nalbuphine, and oxymorphone) which are known to be light sensitive in solution when stored in amber glass HPLC vials. Investigation of the degradation compounds of the same drug product lot of Naloxone HCl Injection (0.02 mg/ml) at two different laboratories in amber glass vials and colourless vials wrapped with foil proved that a Fe$^{3+}$ leaching from the amber glass vials because of Fe oxide was catalysing the degradation. Similar degradation was observed in naloxone, nalbuphine, and oxymorphone that were stored in amber glass. The author conclude that though amber glass are routinely used to protect solutions from light degradation, they should not be used without evaluating effect on sample stability and such leaching has potential to cause degradation of low strength solutions [35].

Silicates

Si is a major glass constituent with other components present in minor proportions to make the glass moldable.
and resistant to temperature changes. Under certain conditions the constituent Si may get leached into the product being stored in it and thus can contaminate the product which upon intravenous administration may produce toxic adverse effects.

Bohrer, et al., investigated the release of Si from glass by interaction with pharmaceutical formulations. The study was carried out by storing separately water (pH from 2-12) and solutions of amino acids, electrolytes, glucose, oligoelements, heparin and sodium bicarbonate in glass containers which were heated at 121°C for 30 min. Si in all the containers was measured using either photometry or atomic absorption spectrometry. The results indicated that even the container with water showed high amounts (0.1 – 1 mg/L) of released Si upon heating. Similar amounts of Si were found in containers with solutions of NaCl, KCl, MgCl₂ and ZnSO₄ and amino acids. Furthermore pH had the greatest influence on amount of leached Si into the product i.e., high pH favors the dissolution of Si. Amount of Si was observed to be higher in solutions of sodium acetate, bicarbonate and gluconate and these results were confirmed by the analysis of commercial products. The authors concluded that release of Si into the product can be enhanced upon sterilization and pH and nature of product decides the extent of release of Si into the product [36].

C. Interaction with Buffers

Buffered and unbuffered products interact differently with glass surfaces. Various buffer systems viz. citrate buffer, tartarate buffer, phosphate buffer etc. are used in parenteral formulations which affects the integrity of glass by different mechanisms.

Bacon, et al., investigated the effect of sodium citrate neutral solutions on sulfur-treated soda-lime glass bottles which inherently are highly resistant towards chemical attacks. Study revealed that the attack on both soda-lime and borosilicate glasses by sodium citrate neutral solutions was very similar to that of attack with highly alkaline solutions. Neutral solution of sodium citrate forms silicon complexes in the range of 5.0 – 7.6, which are soluble in nature and hence, attack by breaking the Si-O-Si structure of glass [37].

Borchert, et al., studied extractables from borosilicate glass containers at accelerated conditions. They used several borosilicate glasses including a mixture of tubing vials, molded vials and ampoules. They used different pH for buffered (pH 8 and 10) and unbuffered (pH 4, 6.5, 8, 9.5, and 10.4) solution for extraction. Extracts were analysed for pH and elemental analysis which includes Si, Na, K, Al, Ba, Ca, Mg, Fe, Zn ions and total extractables. They found high amount of SiO₂ as extractable with solution having high pH, probable reason for this was attack of hydroxyl ions on glass. Na⁺ ions extracted more in acidic solutions, probable reasons for this were dissolution of glass and ion exchange [2].

D. Adsorption of drug(s) or formulation components on glass surfaces

Adsorption of actives from product during storage mainly depends on solute concentration and final product volume. Geary, et al., found that chloroquine which is a 4- aminoquinoline derivative used in malaria therapy binds to higher extent when stored in glass containers and ultimately reduces the bioavailability. Authors have seen up to 40% reduction in chloroquine concentration when stored in glass containers [38].

Ciarlone, et al., studied the binding of tetracyclines with borocilicate glass test tubes in-vitro. They used six tetracyclines namely, chlorotetracycline, demeclocycline, doxycycline, minocycline, oxytetracycline, and tetracycline and all of these bound to borosilicate glass test tubes. Quantitatively highest binding was observed with minocycline. Major factors affecting amount of binding of tetracyclines to glass included time for binding to occur and exposure to increased surface area. They suggested that in case of tetracyclines, containers should be tested for possible binding before use [39].

Song, et al., studied the binding of taxol to glass and plastic containers. Taxol is a natural product having anti-tumor activity. They prepared solution of taxol in 1% methanol in concentrations of 1.8 and 0.18 µg/mL and stored in 1.5 mL flat bottom glass vials and 1.5 mL polypolyethylene tubes at room temperature. After 19 h of storage, the concentration of taxol declined to 40% in 1.5 mL flat bottom glass vials, 55% in 1.5 mL siliconized polypolyethylene tubes and 67% in 1.5 mL unsiliconized polypolyethylene tubes. They concluded that taxol adsorbs rapidly and non-specifically to plastic and glass surfaces [40].

Thakkar, et al., studied the adsorption of hydrophobic amine drug to the container surfaces. They studied the loss of hydrophobic amine α-(di-buty1) amino methyl)-6, 8 dichloro-2- (3', 4'- dichlorophenyl)-4- quinoline- methanol] monohydrochloride due to adsorption on surfaces of different containers. They evaluated glass, polypolyethylene and polyfluoroethylene containers. After 10 h of storage, the concentration of amine declined to 64% in glass beaker, 41% in polypolyethylene beaker and 20% in polyfluoroethylene beaker [41].

Mathes, et al., investigated the influence of the formulation parameters like pH and ionic strength on the IgG adsorption to borosilicate glass vials. They determined that IgG adsorption depended on the formulation pH and ionic strength and to some degree on the type of salt added. The amount of IgG adsorbed resulted from interplay of attractive and repulsive electrostatic interactions between protein molecules and the glass surface as well as among adsorbed protein molecules, the magnitude of each factor varied independently by changing pH and ionic strength. The research showed that in the area of the protein pI, hydrophobic interactions or surface-induced structural changes could occur whereas for pH values below the protein pI, electrostatic interactions are of utmost importance. The amount of salt added could result in either a decrease or increase in the adsorbed amount of protein, depending on whether the protein-surface or intermolecular electrostatic interactions are most pronounced and primarily screened. It was concluded that IgG adsorption on borosilicate glass was mediated to a large extent by electrostatic interactions and less driven by forces such as
hydrophobic interactions or surface-induced structural alterations [42]. Qadry, *et al.*, evaluated the tendency of two proteins to bind to glass vials and CZ-resin vials. The study indicated that the two proteins bound to USP type I glass but not to CZ-resin and thus afforded a suitable alternative to glass for prote. The CZ-resin was found satisfactory for compliance to USP test specifications for extractables however offered no light protection and showed oxygen permeation as well as moisture loss. The moisture less was estimated to be negligible at 5°C which seems to be a typical storage condition for protein formulations. The authors concluded the suitability of CZ-resin vials over glass vials for protein formulations having a potential for adsorption to glass surfaces however also caution that the choice depends upon the type of protein as well as formulation conditions [43].

Eu, *et al.*, studied a method to detect and visualize the adsorption of protein to container surfaces. This study showed that the protein loss, denaturation, or aggregation could occur due to its adsorption to primary containers. The authors applied a gold nanoparticle staining method which involved staining adsorbed proteins with gold nanoparticles to study the adsorption of a therapeutic protein to siliconized glass prefilled syringes. This study also determined that the proteins had affinity to adsorb to glass over siliconized surfaces as well as hydrophobic cyclic olefin polymer plastic vials. Further, the utility of Bovine serum albumin (BSA) to reduce adsorption of the protein to glass was demonstrated [44].

Schwarzenbach, *et al.*, studied the adsorption and adhesion peculiarities of interferon-alpha-2a on glass (Type I and Type I coated) and mica surfaces. Atomic force microscopy was used to directly measure the adhesion forces between interferon molecules and inner surfaces of borosilicate glass vials under aqueous buffer conditions. The authors demonstrated that the adhesion force on Schott FIO-LAX Type I plus was reduced by 40% of the total adhesion force measured on Schott FIO-LAX, a standard type I borosilicate glass quality. The study proved the superiority of the special "Type I plus" coating over undesired protein adsorption to glass [45].

Johnston, *et al.*, acknowledged the potential for recombinant, derived proteins to adsorb to glass and polymeric materials used in their packaging. Their study investigated the role of select solvent additives like glycerin, pluronic F-127, pluronic F-68, tween 80 and tween 20 at different concentrations to reduce the adsorption of a model protein, namely, recombinant human granulocyte colony stimulating factor (rhG-CSF) to glass, polyvinyl chloride (PVC), and polypropylene. The rate of adsorption of rhG-CSF to PVC was extremely rapid. Using viscometry, an estimate of the thickness of the adsorbed layer of rhG-CSF to glass was determined to be approximately 1 micron. The overall rank order of the solvent additives for minimizing adsorption of rhG-CSF to PVC was Tween 20 > Tween 80 > Pluronic F-127 > Pluronic F-68. Tween 20 was found to be most effective solvent additive for inhibiting surface adsorption of rhG-CSF [46].

Mitrano, *et al.*, studied the physicochemical factors that could account for insulin adherence to type I glass bottles from admixtures of insulin with 5% dextrose (D5W) and 0.9% sodium chloride (NS) injections. Factors studied were surface area and volume of the glass bottles. Appropriate volumes of insulin were D5W and NS to yield different dilutions of insulin so that the effect of concentration of insulin could be inferred. KCl Injection was added to mixture of insulin and D5W or NS to study the effect of difference concentrations of KCl. All samples were assayed by gamma scintillation. A direct relationship was found between the percentage of insulin (250 U/L) adhering and the container surface area. It was observed that when the admixture of insulin and D5W at varying fill volumes was filled into the same container, the amount of insulin getting adsorbed to the glass surface decreased, the observation was similar at three bottle sizes of 200, 250 and 500 ml. The observation of decreased adsorption however was seen only with the 250 ml bottle with an admixture of insulin and NS. Increases in insulin concentration though at differing concentrations lead to a decreased adherence in D5W as well as NS admixtures. Thus, the choice of glass bottles so as to have a full bottle could potentially reduce adsorption. KCl contributed to lowering the adherence of insulin in D5W admixture however did not contribute significantly in NS admixture and thus could potentially be used to decrease adsorption of insulin to glass where therapeutically appropriate [47].

**CONCLUSION**

Glass is the most widely used packaging material for parenteral formulations. Glass has been used since a long time in the pharmaceutical industry, significant amount of research and studies are available which indicate the advantages as well as the disadvantages of glass. Lot of data is available which indicates the probable mechanisms of interaction of glass with drug products and such data should be utilized to predict possible adverse interactions so as to enable alternative choices of packaging material or make amendments in the glass type or the formulation. Although we have discussed certain incompatibilities and interactions of the product with glass, it still remains the preferred choice as compared to other packaging materials due to its comparative inertness as well as processing ease for parenteral formulations. Thus, despite the potential for glass to interact, it is a good material of construction for primary containers for parenteral formulations if formulation scientists evaluate and eliminate possible interactions early in the formulation development phase.

**REFERENCES**
